

High Resolution Electronic Measurements in Nano-Bio Science

# **Electrical measurements in liquids** *Basic considerations*

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#### Outline

- Example of electrical measurements in liquid
- The electrical behavior of the (bulk) liquid
- Metal liquid interface: charge redistribution
  - Double-layer capacitance

Next lessons:

- Charge transfer at the metal-liquid interface
- The importance of the mass transport

#### **Example 1**

<u>Oil</u>



### Example 2

#### **Distilled water**



- Parallel plate electroo A<sub>el</sub>= 1cm x 1cm L= 1mm
- Low frequency: resistive behavior
  - High frequency: capacitive behavior

#### **Example 3**

#### Tap water



 $A_{el}$ = 1cm x 1cm L= 1mm

- Low frequency: ≈capacitive behavior
- Medium frequency: resistive behavior
- High frequency: capacitive behavior

#### The role of the ions

Oil



The main difference is given by the number of charge carriers

Ions
 • Charged particles

#### **Nonionic liquids**

#### No ions or charged particles



Non-polar molecule (oil)

#### **Nonionic liquids**



Non-polar liquids have commonly a low dielectric constant ( $\epsilon_r \approx 1.5 - 4$ )

#### **Nonionic liquids**



# Ex. of electrical meas. of nonionic liquids Liquid level sensors



$$C_{meas} \approx \frac{W}{L} \left[ \epsilon_{liq} \, \mathbf{h} + \epsilon_{air} \, (\mathbf{d} - \mathbf{h}) \right] = \frac{W}{L} \left( \epsilon_{liq} - \epsilon_{air} \right) \mathbf{h} + \frac{W}{L} \epsilon_{air} \mathbf{d}$$

No specific instrumentation or measurement technique

#### Ex.: analysis of suspended particles



 $\begin{array}{ll} C_{\text{liquid only}} = \epsilon_{\text{l}} \cdot S & \epsilon_{\text{l}} \text{ dielectric constant of the liquid, S geometrical factor} \\ C_{\text{liquid+particles}} = \epsilon_{\text{e}} \cdot S & \rightarrow & \epsilon_{\text{e}} = \epsilon_{\text{l}} C_{\text{liquid+particles}} / C_{\text{liquid only}} \end{array}$ 

For small particles (<10 $\mu$ m, effective medium theory):

$$f\frac{\epsilon_p - \epsilon_e}{\epsilon_p + 2\epsilon_e} = (1 - f)\frac{\epsilon_l - \epsilon_e}{\epsilon_l + 2\epsilon_e}$$

*f*= volume fraction

- $\epsilon_{\rm p}$  dielectric const. of particles
- 1925 (Fricke, Morse): cell membrane thickness (4nm!)
- dipole moment of molecules [Thompson, J. Chem. Educ., 1966]

# Electrical meas. of biological samples

- ~65% of body mass is water
- Cells, enzymes, proteins,...
  ... "survive" only in water
  <u>+ a lot of ions</u>





#### ...must operate with ionic solutions (electrolytes)!

## Electrolytes

Liquid (water)+ ions







# Electrolytes

Liquid + ions

#### **Conductive behavior**

charge transport



# Electrolytes

Liquid + ions

**Conductive behavior** 

charge transport



## Charge Transport

Diffusion

 $\propto \frac{\partial C_i(x)}{\partial x}$  (*C<sub>i</sub>* concentration)

Drift (migration)

 $\propto C_i E(x)$  (*E* electric field)

- Convection (fluid motion)
  - Natural (density gradient)
  - Mechanical (stirring, flow in microfluidic channel...)

 $\propto C_i v(x)$  (*v* velocity of sol.)

Diffusion Migration  $(\mathbf{f})$ Convection

Wang, Analytical Electrochemistry

#### **Drift current**

Current density due to the charged species i:

 $J_i = z_i q p_i \mu_i E(x)$ 

- $z_i$  = number of charge (dimensionless) of species i
- q= elementary charge (1.6  $10^{-19}$  C)  $\mu_i$  = mobility [cm<sup>2</sup>/Vs] E(x) = electric field [V/cm]

 $p_i = \text{concentration in #ions/cm}^3 = C_i \cdot N_{Av} / 1000$ 

 $N_{Av}$ =Avogadro const.  $N_{Av}$ ≈ 6·10<sup>23</sup> ions/mole

all charged species

 $I_{TOT} = \sum_{i} A J_i$ 

A= surface

C<sub>i</sub>= *molar concentration* = mol / liter

$$J_i = z_i F \mu_i \frac{C_i}{1000} E(x)$$

= Faraday constant = 
$$q N_{Av}$$

$$\sigma_i = z_i q \ p_i \mu_i = \frac{z_i F \mu_i C_i}{1000}$$

conductivity (1/resistivity)

F

## Mobilities and diffusion coefficients

(low concentration, no interionic interactions)

Ionic mobilities of various ions in water [19]

Cation	Mobility (10 <sup>-4</sup> cm <sup>2</sup> /Vs)	Anion	Mobility (10 <sup>-4</sup> cm <sup>2</sup> /Vs)
$H^+$	36.3	$OH^-$	20.5
Li <sup>+</sup>	4	$\mathrm{F}^-$	5.7
$Na^+$	5.2	Cl <sup>-</sup>	7.9
$K^+$	7.6	$\mathrm{Br}^{-}$	8.1
$NH_4^+$	7.6	$I^-$	8.0
Ca <sup>2+</sup>	6.2	$NO_3^-$	7.4
$Mg^{2+}$	5.5	HCO <sub>3</sub>	4.6
La <sup>3+</sup>	7.2	$SO_4^{2-5}$	8.3
$Ag^+$	6.4	$Fe(CN)_6^{3-}$	10.5
$(\widetilde{CH}_3)_4 N^+$	4.7	× 70	
$\mu \approx 5 \cdot 1$	$0^{-4} \frac{cm^2}{Vs} \qquad D$	$P \approx 10^{-5} \frac{cm^2}{s}$	Silicon: μ ≈ 1000 cm²/Vs D ≈ 20 cm²/s

#### Equivalent circuit of bulk solution



$$\begin{split} C_{sol} &\propto \epsilon_{liquid} \\ R_{sol} &\propto \rho \propto \frac{1}{\mu \cdot Concentration} \end{split}$$

 $C_{sol}$  and  $R_{sol}$  are geometry-dependent

Parallel plate electrodes, area A

Small disk: diameter d  $\ll$  L



#### **Dielectric relaxation time**





## **Examples of solution**

• pure water:  $pH = 7 \rightarrow C_{\mu+} = 10^{-7} \text{ M} \rightarrow \rho \approx 20 \text{ M}\Omega \cdot \text{ cm}, \epsilon_r \approx 78$ 

$$\Rightarrow \tau_{d} \approx 140 \mu \text{s}, \quad f_{d} \approx 1 \text{ kHz}$$

• tap water:



 Phosphate Buffered Saline (PBS) commonly used for *in-vitro* biological research

Dulbecco's formula: 137mM NaCl; 8.10mM Na<sub>2</sub>HPO<sub>4</sub>; 2.68mM KCl;...

1M means N<sub>A</sub>= 6.10<sup>23</sup> molecules per liter  $\rightarrow \approx 10^{20}$  ions/cm<sup>3</sup> !

$$\rho \approx 60 \ \Omega \cdot \text{ cm}, \ \varepsilon_r \approx 78$$

same  $\rho$  of silicon doped with  $\approx 10^{14}$  cm<sup>-3</sup> moderate conductor for electronics

$$rac{1}{r}$$
  $\tau_{d} \approx 0.5 \text{ns}$ ,  $f_{d} \approx 350 \text{ MHz}$ 

#### **Electrical current in electrolytes**





#### **Metal-liquid interface**



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## Charge redistribution at the interface



interface electric field: 10-100MV/cm!!!

## **Electrical Model (Stern model)**

Restriction to the closest approach of ions



IHP (≈0.2nm): inner Helmholtz plane: specifically adsorbed ions (bond formation / desolvated)

OHP (≈0.4nm) outer Helmholtz plane: minimum distance of solvated ions (nonspecifically adsorbed, only electrostatic force)

Diffuse layer ( $\approx$ 1-10nm): distribution of ions from OHP to bulk due to thermal motion

#### **Compact layer capacitance**

Restriction to the closest approach of ions



#### **Diffuse layer capacitance**

Ion concentration determined by Boltzman statistics + Poisson eq.



$$\frac{\tanh(zq\phi/4kT)}{\tanh(zq\phi_0/4kT)} = \exp\left(-\frac{x}{L_D}\right)$$

zq= charge of the single ion  $\phi_0$ = potential drop across the diffuse layer (V-V<sub>zero charge</sub>)

> for  $\phi_0 < 50mV$ :  $\phi(x) \cong \phi_0 \exp(-x/L_D)$

$$L_D = \sqrt{\frac{\epsilon kT}{2z^2 q^2 C_0}}$$

Debye length diffuse layer "thickness"

 $C_0$  = ion concentration in the bulk

#### **Diffuse layer capacitance**

Ion concentration determined by Boltzman statistics + Poisson eq.



#### **Diffuse layer capacitance**





depends on the potential ( $\Phi_0$ ) and concentration ( $L_D$ )

#### **Electrical Model (Stern model)**



## **Double layer capacitance**



Potential (V vs NCE)



PBS:

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FIGURE 1-13 Double-layer capacitance of a mercury drop electrode in NaF solutions of different concentrations. (Reproduced with permission from reference 5.)

Wang, Analytical Electrochemistry

C<sub>H</sub> depends on potential, saturated dielectric, ion-ion interaction, adsorption,...

# Well-defined electrode surface

#### Strong sensitivity to the atomic structure of the surface !



# «Real area» of an electrode

#### C<sub>dl</sub> depends on the first few nm of the interface (e.g. in PBS)



Double layer follows hills and valleys having size  $\gg$  Debye length  $\downarrow$ 

nanoscale area of  $C_{dl}$  could be 2-3 times the macroscopic "geometrical area"

#### Atomic scale disorder







distribution of time constants

$$\frac{1}{Z} = Y = \sum_{i} \left( R_i + \frac{1}{sC_i} \right)^{-1}$$

#### **Constant Phase Element**



"Slope" of C<sub>dl</sub> is less than 1 (n = 0.8-0.9) U $Z_{CPE} = \frac{1}{Q(j\omega)^n}$ surface disorder, porous electrodes,

adsorption, ...

Excellent for fitting experimental data (no clear physical insight)

#### **CPE: Look at the Phase**



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### Summary

 Ions make the liquid a conductor: very small mobility (≈ 5.10<sup>-4</sup> cm<sup>2</sup>/Vs), but the ion concentration could be high (PBS: 10<sup>20</sup> ions/cm<sup>3</sup>)

• 
$$R_{solution} = \rho \cdot \text{geometrical factor}, C_{solution} = \varepsilon / \text{geom. factor}$$
  
 $1/\rho = \sum z_i q \ p_i \mu_i = \sum z_i q \ \frac{N_{av}C_i}{1000} \mu_i, \quad \varepsilon = 78 \text{ (water)}$ 

- Resistive behavior up to frequency ≈ 1/(2πρε) physiological solution (PBS) is a "reasonable" conductor up to ≈350MHz
- Metal-liquid interface: a complex charge redistribution
  → double-layer capacitance
- $C_{dl}$  has an enormous value (PBS: 10-40 $\mu$ F/cm<sup>2</sup>)
- Double layer is sensitive to the roughness and atomic structure of the surface  $\rightarrow C_{dl}$  is not a very well-controlled value
- In many practical cases,  $C_{dl}$  is an imperfect capacitor

→ constant phase element:  $Z_{CPE} = \frac{1}{Q(j\omega)^n}$ 

## Small signal equivalent model



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